

## Multi-compartment Model

①

(Delayed distribution Models).

- 1-comp. model → ph. kinetics of many drugs
  - Instantaneous distn' eq. decline in the amount of drug in the body w/ time expressed by mono-exponential term (i.e. elimination).
- Instantaneous distn' is not truly possible for larger no. of drug & drug distn' is not mono-exponential but bi (or) multi-exponential.
- Becoz, body is composed of a heterogeneous group of tissues. Each c diff. degree of blood flow + affinity for drug, so diff. rates of eq'n.

### Assumptions:

1. Blood / plasma & highly perfused tissues such as brain, heart, lung, liver & kidneys as Central compartment.
2. Other tissues & similar distn' → pooled in Peripheral comp't.
3. Intravenous admin. medications → introduced directly into Central comp't.
4. Ir-reversible drug elimination, either by hepatic bio-transformation or renal-excretion, takes place only from the Central comp't.
5. Reversible distn' betw. Central & Peripheral comp't.
6. After Eq. betw. C & P comp't → elimination of drug follows 1-order kinetics.
7. All rate process involving passage of drug in and out of the individual comp't are 1-order process.

8. The peripheral compartment is usually inaccessible to direct measurement & it's not a site of drug elimination clearance.

⇒ Multi-compartment characteristics of a drug are best understood by giving it as I.V. bolus & observing the manner in which plasma concn. declines w.r.t time.

→ Two-compartment Open Model:

→ In this model, body tissues are classified into 2 categories

1. Central compartment or Compartment-1:

comprising of blood & highly perfused tissues like Liver, lungs, kidneys, that equilibrate w.r.t the drug rapidly.

→ Elimination usually occurs from this compartment.

2. Peripheral (or) Tissue Comp. (or) Comp-2:

comprising of poorly perfused and slow equilibrating tissues i.e., muscles, skin, adipose etc.

⇒ classification of a particular tissue: ex: Brain → depends on p.h. proportion of drug.

a) A highly lipophilic drug (alcohol, nicotine, caffeine) can cross BBB → Brain at central compartment.

b) polar drugs, ( $\beta$ -lactam Antibiotics, aminoglycosides) cannot penetrate the BBB → Brain at peripheral compartment.

→ The plasma concn. for a drug that follows a 2-compartment model ④

declines biexponentially as the sum of 2 first-order processes i.e., dist<sup>n</sup> + Elmn.

⇒ Depending upon the compartment from which the drug is eliminated, the 2-compartment model is categorized into 3 types,

1. 2-compartment model w/ Elimination from Central compartment.

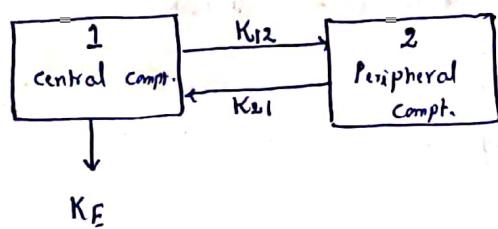
2. " " " " " Peripheral compartment.

3. " " " " " both the compartments.

Two-compartment - Open Model:

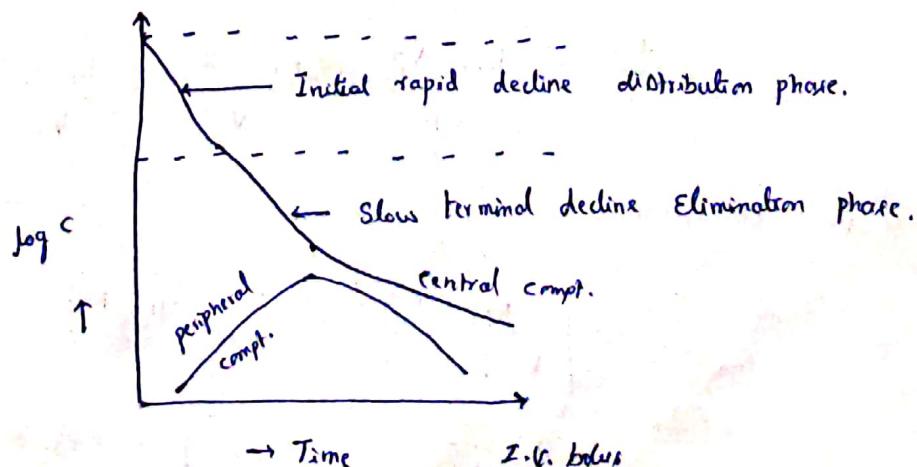
Intravenous Bolus Administration:

Model:



→ After I.V. bolus → Decline in plasma concn is biexponential

indicating the presence of 2 disposition processes viz. distribution and elimination.



Central compt:  
 Initially, the concentration of drug in the central compartment declines rapidly, this is due to distn. of drug from the central comp. to Peripheral comp.  $\Rightarrow$  Distribution Curve.

$\Rightarrow$  After some time, a Pseudo-distr. eq. betw. 2 compd; Subsequent loss of drug from the Central comp. is slow & mainly due to Elimination. This Second, slower rate-process is called as post-distribution (or) Elimination phase.

### Peripheral comp:

(Drug concn, first increases - reaches maximum and declines.  
 (distn) (post distrn / elm).

$\Rightarrow K_{12}, K_{21} \rightarrow$  first-order distrn. rate constants.

$\Rightarrow$  rate of change in drug concn.

$$\frac{dc}{dt} = \text{rate in} - \text{rate out}$$

$\Rightarrow$  rate of change in drug in central comp.,

$$\frac{dc_c}{dt} = K_{21} \cdot C_p - K_{12} \cdot C_c - K_E \cdot C_c$$

$$\Rightarrow V_d = \frac{X}{C}; \quad C = \frac{X}{V_d},$$

$X_c, X_p \rightarrow$  anti-g drug

$$\frac{dc_c}{dt} = \frac{K_{21} \cdot X_p}{V_p} - \frac{K_{12} \cdot X_c}{V_c} - \frac{K_E \cdot X_c}{V_c} \quad V_c, V_p - \text{apparent vol. of dis.}$$

upon Integration.

$$C_c = \frac{X_0}{V_c} \left[ \left( \frac{K_{21} - \alpha}{\beta - \alpha} \right) \cdot e^{-\alpha t} + \left( \frac{K_{21} - \beta}{\alpha - \beta} \right) \cdot e^{-\beta t} \right]. \rightarrow \text{Eq-①.}$$

$X_0 \rightarrow$  I.V. bolus dose!  $\alpha, \beta \rightarrow$  hybrid 1-order compnt.  
 $\hookrightarrow$  depends on  $K_{12}, K_{21}, K_E$ .

∴ Rate of change in drug concn. in Peripheral compartment.

$$\frac{dC_p}{dt} = K_{12} \cdot C_c - K_{21} \cdot C_p.$$

$$= \frac{K_{12} \cdot X_C}{V_C} - \frac{K_{21} \cdot X_P}{V_P}$$

upon Integration,

$$C_p = \frac{X_0}{V_p} \left[ \left( \frac{K_{12}}{\beta - \alpha} \right) \cdot e^{-\alpha t} + \left( \frac{K_{12}}{\alpha - \beta} \right) \cdot e^{-\beta t} \right].$$

$K_{12}, K_{21} \rightarrow$  micro constants (or) transfer const.

→ Relation betw hybrid (or) micro-constants.

$$\alpha + \beta = K_{12} + K_{21} + K_E.$$

$$\alpha \cdot \beta = K_{21} \cdot K_E.$$

→ Eq. ① in simplified form.

$$C_c = A \cdot e^{-\alpha t} + B \cdot e^{-\beta t} \quad A, B \rightarrow \text{hybrid constants.}$$

$C_c$  = distribution exponent + Elimination exponent.

$$A = \frac{X_0}{V_C} \left[ \frac{K_{21} - \alpha}{\beta - \alpha} \right] \Rightarrow C_0 \left[ \frac{K_{21} - \alpha}{\beta - \alpha} \right]$$

$$B = \frac{X_0}{V_C} \left[ \frac{K_{21} - \beta}{\alpha - \beta} \right] \Rightarrow C_0 \left[ \frac{K_{21} - \beta}{\alpha - \beta} \right].$$

$C_0 \rightarrow$  plasma drug concn. immediately after I.V. injection.

Method of Residuals: → To resolve into individual exponents.

$$C_c = A \cdot e^{-\alpha t} + B \cdot e^{-\beta t}$$

→ Initial rapid distn >> terminal elimination.

$\alpha \gg \beta$ ; hence  $e^{-\alpha t}$  approaches zero much faster than  $e^{-\beta t}$ .

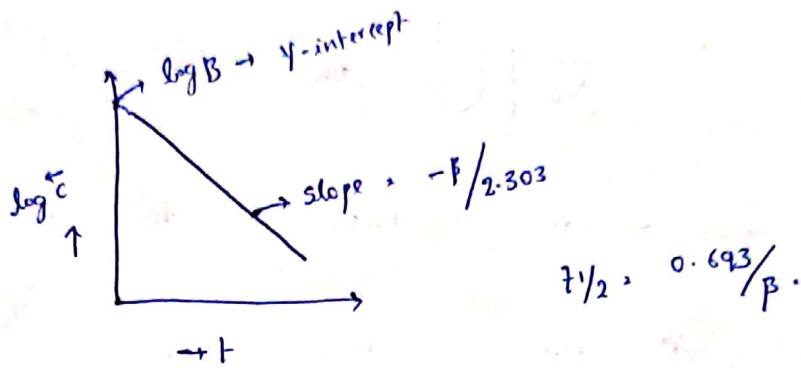
→ Equation reduces to

$$\bar{C} = B \cdot e^{-\beta t}$$

log form:

$$\log \bar{C} = \log B - \frac{\beta t}{2.303}$$

$\bar{C}$  → back extrapolated plasma concn. values.



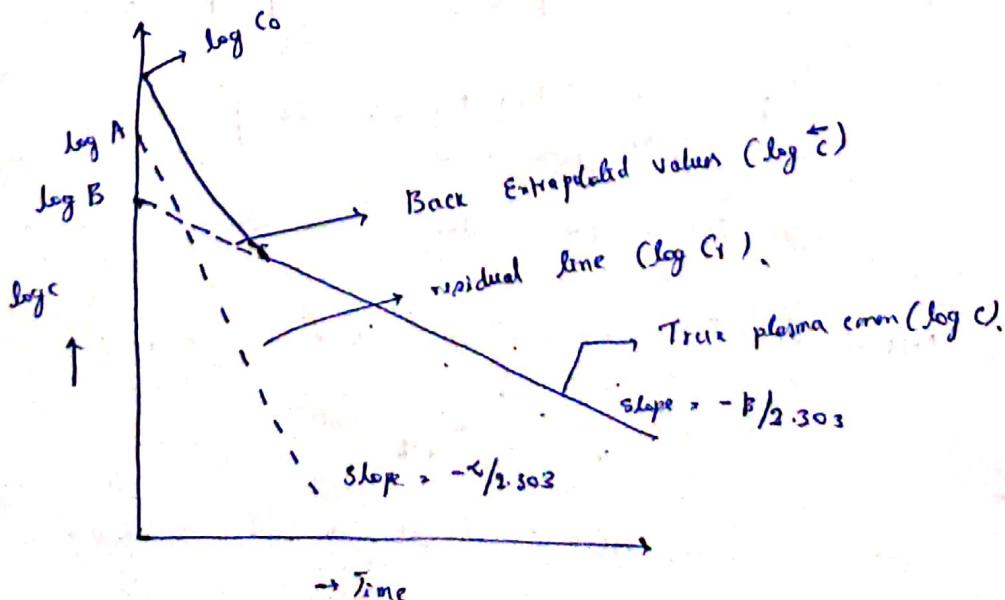
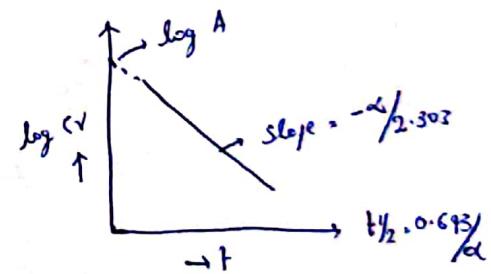
→ Subtraction of Extrapolated plasma concn. values from true plasma concn., yields a residual concn. values  $C_r$ .

$$C_r = C - \bar{C}$$

$$C_r = A \cdot e^{-\alpha t}$$

log form:

$$\log C_r = \log A - \frac{\alpha t}{2.303}$$



→ Assignment of ph. kinetic Parameters:

(1)

- By method of residuals  $\rightarrow A, B, \alpha, \beta \rightarrow$  values needed.
- other parameters  $\rightarrow K_{12}, K_{21}, KE$  (proper substitution).

$$C_0 = A + B$$

$$KE = \frac{\alpha \cdot \beta \cdot C_0}{A\beta + B\alpha}$$

$$K_{21} = \frac{A\beta + B\alpha}{C_0}$$

$$K_{12} = \frac{A \cdot B \cdot (\beta - \alpha)}{C_0 (A\beta + B\alpha)}$$

→  $KE \rightarrow$  Elimination rate const from the Central comp.

$\beta \rightarrow$  . . . . . - Entire Body.

overall Elm.  $t^{1/2}$ , calculable from  $\beta$ .

$$AUC = \frac{A}{\alpha} + \frac{B}{\beta}$$

→ Apparent vol. of central comp.  $V_C$ ,

$$V_C = \frac{X_0}{C_0} = \frac{X_0}{KE \cdot AUC}$$

→ Apparent vol. of peripheral comp.,  $V_P$ ,

$$V_P = \frac{V_C \cdot K_{12}}{K_{21}}$$

→ At steady state

$$V_{d,ss} = V_C + V_P$$

$$V_{d,avg} = \frac{X_0}{B \cdot AUC}$$

→ Total systemic clearance;  $C_L = \beta \cdot V_d$ .

Renal clearance,  $C_L = K_e \cdot V_c$ .

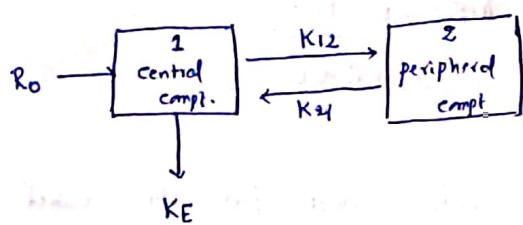
⇒ ph. kinetic parameters → calculated by urinary excretion data,

$$\frac{dx_u}{dt} = K_e \cdot V_c.$$

→ rate of excretion,

$$\frac{dx_u}{dt} = K_e \cdot A \cdot e^{-\alpha t} + K_e \cdot B \cdot e^{-\beta t}.$$

## B. Intravenous Infusion:



→ The plasma C(t) Central compartment, I.V. infusion (zero-order),

$$C = \frac{R_o}{V_c \cdot K_E} \left[ 1 + \left( \frac{K_F - \beta}{\beta - \alpha} \right) \cdot e^{-\alpha t} + \left( \frac{K_E - \alpha}{\alpha - \beta} \right) \cdot e^{-\beta t} \right]$$

→ At steady-state, the second + third term in bracket become zero,

$$C_{ss} = \frac{R_o}{V_c \cdot K_E}$$

Now,  $V_c \cdot K_E = V_d \cdot \beta$ ;

$$C_{ss} = \frac{R_o}{V_d \cdot \beta} = \frac{R_o}{C_L}$$

→ The loading dose  $x_{0,L}$ .

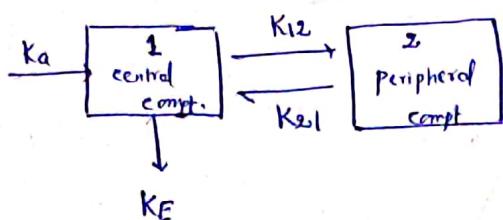
$$x_{0,L} = C_{ss} \cdot V_c = \frac{R_o}{V_c \cdot K_E} \cdot V_c$$

$$x_{0,L} = \frac{R_o}{K_E}.$$

→ Two-Compartment - Open Model:

Extra Vascular      Administration: - First-order      Absorption

Model:



→ The rate of change in drug concn. in central comp is described by

3 exponent → Absorption exponent

Distribution

Elimination

→ The plasma concn;

$$C = N \cdot e^{-\alpha t} + L \cdot e^{-\beta t} + M \cdot e^{-\gamma t}$$

$C = A_{abs} \text{Expt} + A_{dist} + Elm.$

L, M, N - co. efficients.

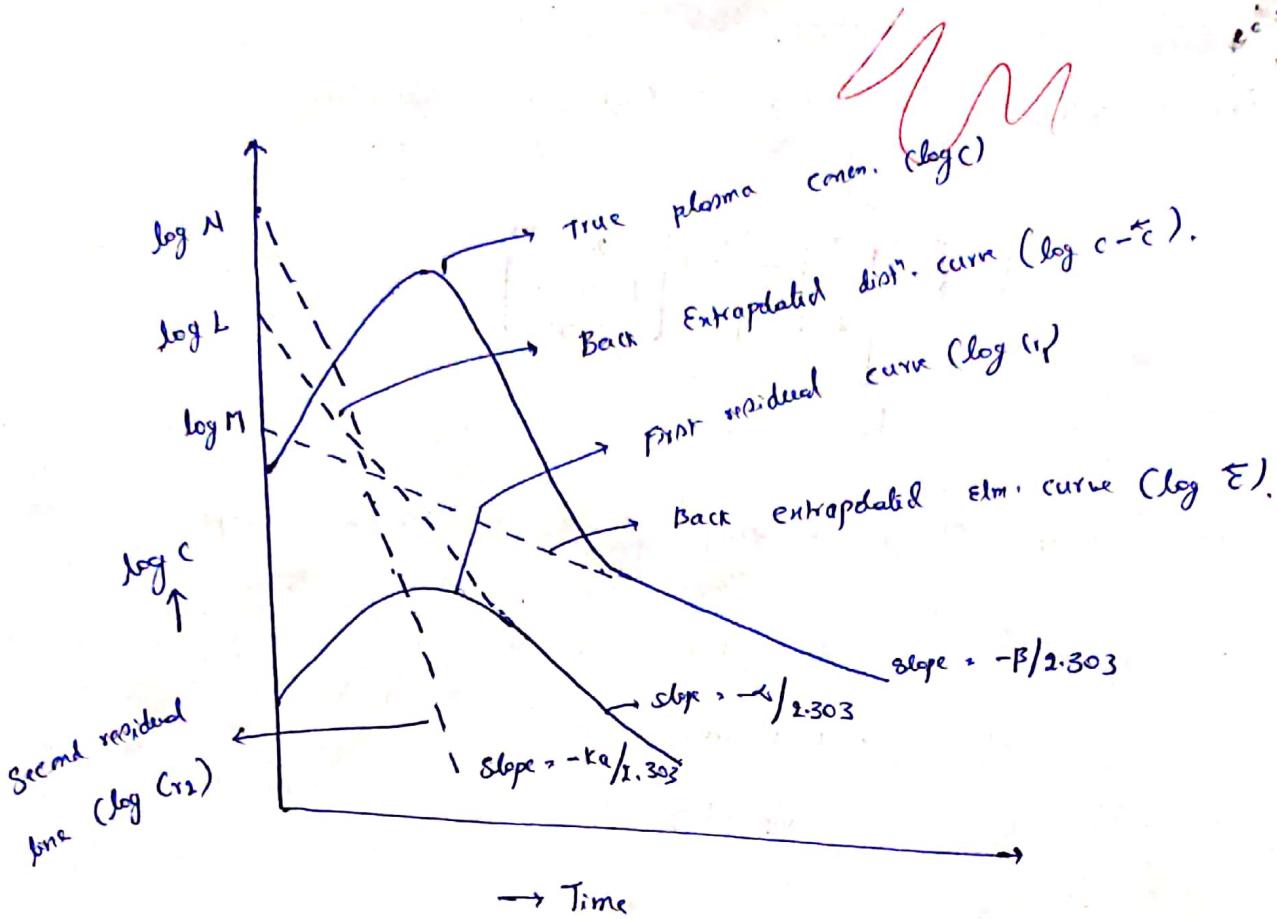
1) → method of residuals,  $K_a > \alpha > \beta$ .

2) Zee-Riegelman method →  $K_a$  estimation,

(contrast to Wagner-Nelson method).

→ Method requires plasma-time data profiles after oral and I.V. admin. of the drug to the same subject at diff times.

→ The method can be applied to drugs that distribute in any number of compartments.



### Three-compartment model:

